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An elastase activity reporter for Electronic Paramagnetic Resonance (EPR) and Overhauser-enhanced Magnetic Resonance Imaging (OMRI) as a line-shifting nitroxide


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ABSTRACT

Pulmonary inflammatory diseases are a major burden worldwide. They have in common an influx of neutrophils. Neutrophils secrete unchecked proteases at inflammation sites consequently leading to a protease/inhibitor imbalance. Among these proteases, neutrophil elastase is responsible for the degradation of the lung structure via elastin fragmentation. Therefore, monitoring the protease/inhibitor status in lungs non-invasively would be an important diagnostic tool.

Herein we present the synthesis of a MeO-Suc-(Ala)2-Pro-Val-nitroxide, a line-shifting elastase activity probe suitable for Electron Paramagnetic Resonance spectroscopy (EPR) and Overhauser-enhanced Magnetic Resonance Imaging (OMRI). It is a fast and sensitive neutrophil elastase substrate with $K_m = 15 \pm 2.9 \mu M$, $k_{cat}/K_m = 930,000 \text{ s}^{-1} \text{ M}^{-1}$ and $K_m = 25 \pm 5.4 \mu M$, $k_{cat}/K_m = 640,000 \text{ s}^{-1} \text{ M}^{-1}$ for the R and S isomers, respectively. These properties are suitable to detect accurately concentrations of neutrophil elastase as low as 1 nM. The substrate was assessed with broncho-alveolar lavages samples derived from a mouse model of Pseudomonas pneumonia. Using EPR spectroscopy we observed a clear-cut difference between wild type animals and animals deficient in neutrophil elastase or deprived of neutrophil Elastase, Cathepsin G and Proteinase 3 or non-infected animals.

These results provide new preclinical ex vivo and in vivo diagnostic methods. They can lead to clinical methods to promote in time lung protection.

1. Introduction

Pulmonary inflammatory diseases represent a major health concern worldwide as well as an economic burden. They include asthma, cystic fibrosis (CF), chronic obstructive pulmonary disorder (COPD) (e.g., emphysema), acute respiratory distress syndrome and alpha-1-antitrypsin deficiency. For instance, COPD alone concerns a population estimated to 175 million people and accounts for 3.2 million deaths ranking it to the fifth cause of mortality worldwide [1]. Among the precipitating factors for disease development are tobacco smoking, urban air pollution and wood fire smoke. A common denominator of pulmonary inflammatory diseases is the high neutrophil influx as seen in CF or during the exacerbation phase of COPD. At inflammation sites, neutrophils discharge four serine proteases into the extracellular environment whose concentrations surpass that of their corresponding physiologic inhibitors resulting in protease/anti-protease imbalance.
causing tissue damage, hence progressive loss of lung functions.

Neutrophil elastase (NE), a potent protease, was shown to be the main tissue-destructive actor because of its large repertoire of substrate including structural proteins particularly elastin [2,3], a major lung structural protein, although the four neutrophil proteases can act synergistically [4].

Therapeutically, lungs protection needs an adapted treatment with protease inhibitors. However, preclinical research to setup such protocols is impaired by the absence of a reliable imaging method to localize deleterious enzyme activities in order to assess the actual protease/antiprotease balance status before and after treatment. Ultimately, an elastase activity imaging method valid for humans would detect lung inflammation long before any irreversible tissue damage could occur. Thus a treatment with inhibitors [5] or a change in habits could be proposed “in time” to save the lungs.

Molecular imaging of the proteolytic activity is most easily done using internally quenched fluorescent substrates. These substrates have good enzymatic constants because they can encompass both the P and P’ regions in the Schechter and Berger nomenclature [6]. There are however several drawbacks of this method: substrate fluorescence quenching is not complete thus causing long waiting times to eliminate nonspecific “blinding” light, light tissue penetration is limited and prevents imaging of deeply seated tissues or skull and three-dimentional images are obtained by reconstruction.

Magnetic Resonance Imaging (MRI) methods have a superior true 3D space encoding and use wavelengths that only weakly interfere with tissues. Electronic Paramagnetic Resonance (EPR) is a sensitive free radical detection method suitable in visible light-opaque media. Stable free radicals such as nitroxides or trityls can be detected or imaged in vitro and in vivo. Since unpaired electrons are particularly sensitive to the electronic environment some have been designed to display resonance line broadening or shifting to detect various parameters. Hence free radicals have been used for oximetry [7,8], redox status imaging [9,10], pH measurement [11–14], water content measurement [15] or to report on enzymatic activity [16–18]. EPR imaging (EPRI) can be used with these free radicals. Unfortunately, due to the very fast relaxation of free electrons EPR still remains slow and insufficiently resolved. Magnetic Resonance Imaging (MRI) is the method of choice to deliver exquisite anatomical details but its low sensitivity so far prevented molecular imaging such as enzyme activity imaging. Interestingly, a line shifting substrate can also be monitored by Overhauser-enhanced Magnetic Resonance Imaging (OMRI). OMRI is an emerging imaging method designed to enhance NMR sensitivity. It is a double resonance experiment transferring a part of the higher spin polarization of an unpaired electron to the environing water protons (through the electron-proton Overhauser effect) which enhances the MRI signal that appears brighter [19].

It has been shown recently that OMRI at 0.2 T was able to reveal brain tumors in mice models of glioma through intravenous injection of a nonspecific nitroxide with high contrast on three-dimensional images [20]. Moreover, a nonspecific prototype of the line-shifting nitroxide later described in this study was able to reveal stomach and intestinal enzymatic activity [18] (see reaction in Scheme 1). Both studies showed that high contrast and high resolution images are possible in mice with short recording times.

In this paper the synthesis of MeO-Suc-(Ala)₂-Pro-Val-nitroxide (molecule 3 in Scheme 1), the first of a new family of dedicated protease substrates based on line-shifting nitroxides is reported. Its catalytic properties with neutrophil elastase and various enzymes were studied using EPR spectroscopy.

The substrate was probed in broncho-alveolar lavages from a mouse model of Pseudomonas aeruginosa lung infection with wild type and several mice knocked-out for neutrophil serine proteases.

It is also shown that this substrate is suitable for Overhauser-enhanced Magnetic Resonance Imaging.

![Scheme 1. Enzymatic activity on enol acetate 2 releasing 1. Elastase targeting substrate 3.](image)

2. Material and methods

2.1. Organic synthesis

2.1.1. General remarks

1H nuclear magnetic resonance (NMR) spectra were recorded using an internal deuterium lock at ambient temperatures on the following instruments: Bruker AC 400 (400 MHz) and Bruker AC 300 (300 MHz). Data are presented as follows: chemical shift (in ppm), integration, multiplicity (s = singlet, d = doublet, t = triplet, m = multiplet, br = broad, dd = doublet of doublets), coupling constant (J in Hz) and integration. 31P NMR spectra were recorded on a Bruker AC 300 (122 MHz) and on a Bruker AC 400 (162 MHz) spectrometers with complete proton decoupling. Chemical shifts (δ) were reported in ppm using TMS as internal reference for 1H and 13C NMR spectra, and 85% H3PO4 for 31P NMR spectra. High-resolution mass spectra (HRMS) were performed on a SYNAPT G2 HDMS (Waters) spectrometer equipped with atmospheric pressure ionization source (API) pneumatically assisted. Samples were ionized by positive electrospray mode as follows: electrospray tension (ISV): 2800 V; opening tension (OR): 20 V; nebulization gas pressure (nitrogen): 800 L/h. Low resolution mass spectra were recorded on ion trap AB SCIEX 3200 QTRAP equipped with an electrospray source. The parent ion (M⁺, [M+H]⁺, [M+Na]⁺ or [M+NH₄]⁺) is quoted. Analytical thin layer chromatographies (TLC) were carried out on Merck Kieselgel 60 F254 plates. Flash column chromatographies were carried out on Merck Kieselgel 60 (230–400 mesh). Solvent system: gradients of DCM/MeOH; EtOAc/EtOH. All experiments were performed under anhydrous conditions and an inert atmosphere of argon and, except where stated, using dried apparatus and employing standard techniques for handling air-sensitive materials. For EPR measurements, samples with 0.5 mM concentration of nitroxide were prepared in non-degassed solvents. Experiments were performed indifferently on Elexsys, EMX or ER 100D Bruker machines (a difference smaller than 0.1 G was noticed). EPR spectra were recorded with a gain of 2 105 (72 dB for Elexsys), a modulation amplitude of 1.0 G, a sweep width of 150 G, a sweep time of 21 s, and a power of 20 mW.

2.1.2. (9H-fluoren-9-yl)methyl-(S)-2-(((S)-(1-(benzyloxy)-3-methyl-1-oxobutan-2-yl)carbamoyl) pyrrolidine-1-carboxylate (2)

DPEA (2 mL, 11.5 mmol) was added dropwise to a stirred suspension of i-Val-OBn-HCl (2.8 g, 11.5 mmol) in dichloromethane (30 mL) at room temperature under an atmosphere of nitrogen. On dissolution, the solution was cooled to 0 °C and Fmoc-L-Pro (4.26 g, 12.6 mmol) and 1-hydroxybenzotriazole (1.86 g, 13.8 mmol) were added successively, each in one portion. The suspension was stirred at 0 °C for a further 15 min, and then DCC (2.85 g, 13.8 mmol) was added in one portion. The mixture was allowed to warm to room temperature over the course of...
of 18 h and then filtered, and the filtrate was evaporated in vacuo. The residue was taken up in ethyl acetate and filtered, and the filtrate was then washed with 10% aqueous citric acid solution followed by saturated aqueous sodium bicarbonate solution. The combined organic layers were dried and evaporated in vacuo to afford the crude product which was purified by chromatography on silica using 3:2 petroleum ether–EtOAc as eluent to yield the protected dipeptide 2 (5.94 g, 11.28 mmol) as a light yellow solid (98%). [α]D20 = 50 (c 1.0, CHCl3). 1H NMR (300 MHz, CDCl3) δ 7.68 (d, J = 7.5 Hz, 2H), 7.48 (s, 2H), 7.33–7.17 (m, 9.7H), 6.43 (br s, 0.3H), 5.20–4.82 (br 2H, 2H), 4.48–4.16 (m, 5H), 3.48–3.38 (m, 2H), 2.27–1.86 (m, 5H), 0.80 (d, J = 6.8 Hz, 2H), 0.75 (d, J = 6.6 Hz, 1H). 13C NMR (75 MHz, CDCl3) δ 172.2, 171.6, 156.1, 155.2, 143.8, 141.3, 135.5, 128.6, 128.4, 128.3, 127.8, 127.1, 125.1, 120.0, 67.8, 67.0, 61.2, 60.4, 57.3, 53.5, 47.6, 47.2, 47.0, 33.9, 31.5, 31.2, 28.2, 24.7, 23.7, 19.1, 17.6. HRMS (ESI) calc for C32H35N2O5+: 479.2540 [M+H]+; found: 479.2538.

2.1.5. Methyl (S)-4-((1-(benzyloxy)-1-oxopropan-2-yl)amino)-4-oxobutanoate (6)

To a solution of 7 (7 g, 20.71 mmol) in MeOH (80 mL) was added 10% Pd/C (750 mg), and the mixture was stirred for 10 h in hydrogen atmosphere (1 atm). The reaction mixture was filtered through Celite, and MeOH was removed in vacuo to yield quantitatively the free acid (4.85 g, 28.56 mmol). 1H NMR (300 MHz, CDCl3) δ 175.7, 174.9, 174.7, 174.0, 52.2, 50.1, 49.2, 31.2, 30.0, 18.0, 17.6. HRMS (ESI) calc for C15H22N3O8+: 365.1707 [M + H]+; found: 365.1696.

2.1.6. Methyl 4-(((S)-1-((S)-1-(benzoxyl)-1-oxopropan-2-yl)amino)-1-oxopropan-2-yl)(amino)-4-oxobutanoate (7)

To a solution of 6 (7 g, 23.86 mmol) in MeOH (80 mL) was added 10% Pd/C (700 mg), and the mixture was stirred for 10 h in hydrogen atmosphere (1 atm). The reaction mixture was filtered through Celite followed by MeOH removal in vacuo to yield quantitatively the free acid (4.85 g, 23.8 mmol). DIPEA (14.9 mL, 83.52 mmol) was added dropwise to a stirred suspension of l-Ala-ObnHCl (6.16 g, 28.56 mmol) in dichloromethane (100 mL) at room temperature under an atmosphere of nitrogen. On dissolution, the solution was cooled to 0 °C and the acid obtained in the previous step (4.85 g, 23.8 mmol) and 1-hydroxybenzotriazole (3.86 g, 28.56 mmol) were added successively, each in one portion. The suspension was stirred at 0 °C for a further 15 min, and then DCC (5.89 g, 28.56 mmol) was added in one portion. The mixture was warmed to room temperature in 18 h and then filtered, and the filtrate was evaporated in vacuo. The residue was taken up in ethyl acetate and filtered, and the filtrate was then washed with 10% aqueous citric acid solution followed by saturated aqueous sodium bicarbonate solution. The combined organic layers were dried and evaporated in vacuo to leave the crude product which was purified by chromatography on silica using 3:2 petroleum ether–EtOAc as eluent to afford 7 (7.5 g, 20.71 mmol) as a white solid in 87% yield. [α]D20 = 44 (c 1.0, CHCl3). 1H NMR (300 MHz, CDCl3) δ 7.25 (s, 5H), 7.10 (s, 1H), 6.69 (s, 1H), 5.07 (dd, J = 18, 12 Hz, 2H), 4.58–4.42 (m, 2H), 3.55 (s, 3H), 2.57 (dd, J = 10, 4.0 Hz, 2H), 2.41 (dd, J = 10.4, 4.5 Hz, 2H), 1.32 (d, J = 7.2 Hz, 3H), 1.27 (d, J = 7.0 Hz, 3H). 13C NMR (75 MHz, CDCl3) δ 173.4, 172.4, 172.2, 171.3, 135.5, 128.6, 128.4, 128.1, 67.0, 51.8, 48.8, 48.2, 30.8, 29.2, 18.4, 17.8. HRMS (ESI) calc for C15H22N3O8+: 365.1707 [M + H]+; found: 365.1696.

2.1.7. Methyl-4-(((S)-1-(((2,5-dioxopyrrolidin-1-yl)-Oxy)-1-oxopropan-2-yl)(amino)-1-oxopropan-2-yl)(amino)-4-oxobutanoate (8)

To a solution of 7 (7.5 g, 20.71 mmol) in MeOH (80 mL) was added 10% Pd/C (750 mg), and the mixture was stirred for 10 h in hydrogen atmosphere (1 atm). The reaction mixture was filtered through Celite followed by MeOH removal in vacuo to yield quantitatively the free acid (5.68 g, 20.71 mmol). [α]D20 = 8.7 (c 1.0, CHCl3). 1H NMR (300 MHz, MeOD) δ 4.39 (dd, J = 7.1, 3.1 Hz, 2H), 3.66 (s, 3H), 2.64 (dd, J = 10.1, 4.0 Hz, 2H), 2.52 (dd, J = 10.3, 4.0 Hz, 2H), 1.41 (d, J = 7.3 Hz, 3H), 1.35 (d, J = 7.2 Hz, 3H). 13C NMR (75 MHz, MeOD) δ 175.7, 174.9, 174.7, 174.0, 52.2, 50.1, 49.2, 31.2, 30.0, 18.0, 17.6. HRMS (ESI) calc for C18H26N3O8+: 372.1401 [M + H]+; found: 372.1400.

2.1.8. Synthesis of R-†

A solution of ketone R-† (209 mg, 0.71 mmol) in dry THF (10 mL) was slowly added to solution of LiHMDS (1.0 mol solution in THF, 1.2 mL, 1.21 mmol, 1.70 equiv.) at 78 °C in dry THF (5 mL). The mixture was stirred for 3 h from – 78 °C to – 45 °C. Then, 4 (739 mg, 1.42 mmol, 2 equiv.) was slowly added as a cold (- 45 °C) solution in 10 mL THF. The mixture was stirred for 2.5 h, then it was poured quenched with saturated aqueous NH4Cl solution and extracted with EtOAc. The combined organic extracts were dried with MgSO4, filtered, and concentrated under vacuo. Column chromatography of the residue gave starting material R-† (92 mg, 0.31 mmol) and the targeted product R-*.
2.3. EPR spectroscopy of peptide-nitroxide substrates

All samples were loaded in 75 μL (75 mm) capillaries (BLAUBRAND micropipettes). Acquisitions were performed at 25 °C with a temperature controller (BIO-I, NOXYGEN, Germany) fitted to an EMXnano EPR spectrometer (BRUKER, Germany), under the control of Xenon software (BRUKER). Quantitation of substrate and product nitroxides at each time of the kinetics was done by fitting with both reference spectra using the Spinfit module of Xenon software. Substrate and product concentrations were obtained using the included Spincount calibrated module.

Enzymatic activity assays were carried out using the EPR spectroscopy to monitor the substrate hydrolysis.

2.3.1. Enzymatic specificity screening in vitro

A list of proteases, described in Enzymes section, with various specificities and origins were tested in pursuit of an effective proteolytic activity on the nitroxide. All experiments were done with 1 nM proteases. Enzymatic reactions were initiated by adding a small volume of substrate 25 μM. Kinetics was immediately recorded by EPR during 2 h. EPR acquisition parameters were set as follows: Bo = 3423 G, sweep width = 120 G; sweep time = 10 s, attenuation = 6 dB; delay between scan = 30 s; modulation amplitude = 1 G; gain = 50 dB. Post processing was done with IGOR Pro (Wavemetrics, Lake-Oswego, OR, USA), initial velocities from different enzymes were collected and compared in a histogram.

2.3.2. Michaelis kinetics constants of NE with both peptide-nitroxide isomers

Kinetic reactions were made with NE.1 nM by adding a range of 11 concentrations of substrate from 2.5 μM to 200 μM, prepared temporarily to limit spontaneous hydrolysis. EPR acquisition parameters were set as follows: Bo = 3423 G, sweep width = 120 G; sweep time = 10 s, attenuation = 6 dB; delay between scan = 30 s; modulation amplitude = 1 G; gain = 50 dB. Thus spectra were recorded at 10 s interval. Quantitation of substrate and product nitroxides at each time of the kinetics was done by fitting with both reference spectra using the Spinfit module of Xenon software. Substrate and product concentrations were calculated using the included Spincount calibrated module. Product concentrations were plotted as a function of time. Initial velocities were extracted by linear regression on the linear portion of the plot (less than 5% of substrate consumed) for each initial substrate concentration. Initial velocities values were finally plotted versus substrate concentration. Michaelis-Menten hyperbolic representation was built from the initial velocities and a nonlinear regression analysis was performed using Michaelis-Menten equation: v0 = kcat × [S] / (km + [S]). Enzymatic parameters, Km and kcat were determined for both substrate isomers.

2.3.3. Neutrophil elastase activity in bronco alveolar lavage

Proteolysis was started by adding 1 mM substrate in 30 μL of bronco alveolar lavage (BAL) samples. Samples were then immediately loaded in capillaries. EPR acquisition parameters were set as follows: Bo = 3423 G, sweep width = 120 G; sweep time = 10 s, attenuation = 25 dB; delay between scan = 30 s; modulation amplitude = 1 G; gain = 40 dB. Kinetic reactions were followed for 8 h at 25 °C. All experiments were repeated on 4 or 5 different mice. The resulting slope of progress curves [Product] = f(time) were plotted against the various genotypes in a histogram representation. Results were normalized with the condition WT infected.

2.4. Mouse inflammation model

2.4.1. Generation of mice deficient in CG, NE, and PR3

Simultaneous deficiency of the Prm3 and Ela2 gene clusters (129S6/
SvEv), deficiency in CG (129S6/SvEv-C57BL/6J), and deficiency in NE (129S6/SvEv-C57BL/6J) were generated by targeted mutagenesis as described elsewhere [21–23]. NE-PR3–deficient mice and CG-deficient mice were crossed to generate heterozygote-deficient progeny (F1). The F1 progeny were intercrossed to generate mice deficient in NE, PR3, and CG, referred to as NSP-KO [3]. Mouse strains were subsequently backcrossed (eight generations) on a pure C57BL/6J background. Mice were housed in a pathogen-free facility with food and water ad libitum and a 12-h light/dark cycle.

Animal handling and procedures were approved by the Animal Studies Committee at our institution (Health and Animal Protection Office, Châlons-en-Champagne, France, Authorisation number: 51–31) in accordance with the guidelines of the Federation of European Laboratory Animal Science Associations and following the European Directive 2010/63/EU on the protection of animals used in scientific procedures.

2.4.2. Bacteria and intranasal infection

P. aeruginosa H103 was kindly provided by Dr. Hancock (Vancouver, BC, Canada) [24]. An overnight bacterial culture (1 mL) was grown in Luria Bertani broth (10 mL) at 37 °C to late exponential phase (3 h). Bacteria were washed twice with PBS (pH 7.4) and the optical density (OD) of the cultures was determined at 600 nm (1 OD600 nm = 1 × 10^8 bacteria/mL).

Mice (n = 5 mice/genotype) were challenged intranasally with bacteria and sacrificed at fixed time points. Briefly, mice were anesthetized by intraperitoneal injection of ketamine hydrochloride (75 mg/kg) and medetomidine hydrochloride (1 mg/kg). Next, mice were challenged intranasally with 50 μL of saline buffer (PBS) containing a predetermined sublethal dose of bacteria (10^6 CFUs per mouse) [25]. Control mice (n = 5 mice/genotype) were challenged with 50 μL of sterile PBS alone. WT mice, NE-KO deficient mice and NSP-KO mice were sacrificed at 24 h post-infection. At this time point, mouse lungs were analyzed for inflammatory cell recruitment and detection of free active NE. Of note, all types of mice displayed a morbid impact of electromagnetic HF. Of note, all types of mice displayed a morbid impact of electromagnetic HF.

2.5. OMRI

2.5.1. EPR cavity and MRI system

The OMRI system used in all experiments is an EPR cavity (Bruker, Wissenburg, France) inserted at the center of Cirrus Open 0.2 T MRI (RFPA, Artigues-pres-Bordeaux, France), generated the HF wave. The EPR resonance frequency was around 5.4 GHz, according to the central EPR frequency of the nitroxide of interest. The resonant cavity was tuned and matched with the help of a network analyzer (Agilent Technologies, Santa Clara, CA, USA) at this resonance frequency.

2.5.2. Pulse sequences

2D magnetic resonance images were generated with a Gradient Echo sequence. It was modified to include a continuous EPR saturation during all the acquisition which started 300 ms prior to the first NMR RF pulse. All MR adjustments were done manually, using the same fixed parameters: TE/TR = 20/200 ms, field of view 40 ° 40 mm^2, Matrix size 64 ° 64, flip angle 30°, receiver bandwidth 20 kHz, with and without HF irradiation (S_ON and S_OFF).

2.5.3. Overhauser enhancements and EPR frequency

The EPR irradiation frequency was adjusted on the 4th peak upfield of the EPR spectrum of the nitroxide to have a specific excitation of the nitroxide of interest. Frequency sweep experiments were carried out to characterize OMRI response of substrate and product at 1 mM each. The Overhauser enhancement was calculated as the ratio of the absolute value of the NMR signal-to-noise ratio (SNR) in the presence of electron saturation divided by the SNR measured without electron saturation (S_SN)

The DNP factor (DNPF) is defined as < Iz > /I0−1 where < Iz > stands for the expected value of proton magnetization in the presence of EPR saturation and I0 is the equilibrium proton magnetization. Assuming a steady-state electron saturation, DNPF = (ρfs/ρ0)γ /γ1

where γ2 and γ1 are the electron and proton gyromagnetic ratio, respectively, p the electron-nucleus coupling factor, n the number of EPR lines, s the saturation factor and f the leakage factor. The leakage factor can be expressed as:
f = r1 [c] / (R0 + r1 [c]),

where [c] is the nitroxide concentration, r1 its longitudinal relaxivity and R0 is the proton longitudinal relaxation rate constant in the absence of nitroxide. Due to the negative sign of the electron gyromagnetic ratio and the positive sign of the coupling factor (mostly dipolar in liquids), the Overhauser effect induce an out-of-phase shift of the proton magnetization and thus a negatively signed DNPF. The relationship between the Overhauser enhancement and the DNPF is:

Overhauser enhancement = |DNPF| − 1

DNP factor vs nitroxide concentration were evaluated by curve fitting to Eq. (1) with R1D = 0.4 s⁻¹ and r1 (determined from inversion-recovery experiments) as fixed parameters, and the product s as a floating parameter.

Details on the theoretical background can be found in Overhauser [28], Abragam et al. [29] and a summary is given in Mellet et al. [27]. Overhauser enhancements were finally plotted against EPR frequency and specific irradiation frequency was selected for each nitroxide form (Fig. 6). Lineshape were evaluated from curve fit to a lorentzian function. Nitroxide relaxivity was calculated from inversion-recovery experiments [30]. Inversion times ranged from 10 ms to 10 s. NMR signals vs inversion delay were fitted to a single exponential recovery curve and relaxation rate constants vs nitroxide concentration (0–2 mM range) were adjusted with a linear model.

2.5.4. Kinetic measurements in vitro

OMRI of proteolysis kinetics was performed both by looking at the substrate consumption and by looking at the product formation in separate experiments. Experiments were done in the presence of 40 nM NE (product kinetic) and 20 nM NE (substrate kinetic). Kinetics of hydrolysis were started by adding 0.5 mM substrate (product formation) or 1 mM (substrate consumption). Control experiments were carried out without enzyme. For each nitroxide form, two sets of 2D images were
acquired at various time intervals with and without electron saturation with the imaging parameters described above.

3. Results

3.1. Synthesis of the methoxy-succinyl-alanine-alanine-proline-valine-nitrooxide enol ester

As mentioned above, nitroxides 1•/2• exhibit high potential to investigate proteolysis both by EPR and OMRI. Recently, enantiomers of 1• were separated, identified and, then used for the preparation of the peptide-nitroxide substrate (reported elsewhere [31]).

After applying a similar approach, (details of the synthesis modifications are published elsewhere [31]) peptide-nitroxides R-3• and S-3• putatively specific of neutrophil elastase protease were prepared in two steps (Scheme 2 and Material and Methods section), in the first step, the condensation of the activated peptide 4 (Scheme 3A and see Material and Methods section) with the enolate of R-1• to yield nitroxide R-4•, and, in the second step, coupling of R-4• with the activated peptide 8 (Scheme 3B) to afford R-3•. The same procedure was applied to S-1• to yield S-3• (overall yield of 45%, see Material and Methods section).

Activated peptides 4 and 8 were prepared according to conventional procedures (Scheme 3A and B). That is, using the standard DCC procedure Fmoc-protected L-proline group, than with the widely used paranitroanilide leaving group, as the peptide that fills the P part was identical in the two substrates.

3.2. Enzyme kinetics of substrate to product hydrolysis by NE

3.2.1. Enzymatic hydrolysis of the substrate

Chemical structures of substrate and enzymatic reaction product are illustrated in Scheme 4.

As a preliminary experiment, the kinetics of hydrolysis of the substrate by neutrophil elastase was studied by EPR (Fig. 1). The EPR parameters including nitrogen and phosphorus hyperfine coupling constants (aN and aP respectively) as they appear before and after hydrolysis of substrate in the presence of NE are reported in Table 1.

As described in Table 1, product’s linewidth was 1.22 G while substrate’s linewidth was 1.84 G. Thus, for EPR spectroscopy measurements the product will show a better sensitivity and for Overhauser-enhanced MRI specific excitation of the product will provide a greater signal enhancement compared to the substrate as outlined hereafter.

3.2.2. Determination of the Michaelis constants

Kinetics of consumption of substrate and formation of product were monitored in the concentration range of 2.5–200 μM (Fig. 2).

Initial velocities were deduced from the slope of each progress curve displayed in Fig. 2. Finally, Michaelis-Menten plots (Fig. 3) allowed us to determine Michaelis constants (Table 2).

Kinetic constants for R-3• derived from these measurements are Km = 15 μM and kcat = 14 s⁻¹, indicating a catalytic efficiency, kcat/Km of 940 000 s⁻¹ M⁻¹. Constants for S-3• are Ks = 25 μM and kcat = 16 s⁻¹, with kcat/Km of 640 000 s⁻¹ M⁻¹. Both isomers thus display similar kinetic constants, having a Ks ≈ 7 fold lower than that of the reference chromogenic substrate MeO-Suc-(Ala) Pro-Val-pNA and a catalytic constant 6–9 fold higher [35]. These results suggest that better interactions occur with the P’ part of the substrate, namely the nitroxide group, than with the widely used paranitroanilide leaving group, as the peptide that fills the P part was identical in the two substrates.
hyperfine coupling of the unpaired electron with the phosphorus atom $^{31}P$ (spin $\frac{1}{2}$) and with the nitrogen atom $^{14}N$ (spin 1) provide 6 EPR lines. Parameters $a_P$ and $a_N$ are phosphorus and nitrogen coupling constants deduced from EPR product or substrate spectra. (For interpretation of the references to color in this figure legend, the reader is referred to the web version of this article.)

**Table 1**

<table>
<thead>
<tr>
<th>Nitroxides</th>
<th>$a_P$ (G)</th>
<th>$a_N$ (G)</th>
<th>$g^{(i)}$</th>
<th>Linewidths (G) $^{(b)}$</th>
</tr>
</thead>
<tbody>
<tr>
<td>Substrate</td>
<td>15.5</td>
<td>38.4</td>
<td>2.0052</td>
<td>1.84</td>
</tr>
<tr>
<td>Product</td>
<td>14.9</td>
<td>43.3</td>
<td>2.0053</td>
<td>1.22</td>
</tr>
</tbody>
</table>

3.2.3. **Specificity screening of the substrate**

Enzyme specificity screening was carried out in vitro. Initial velocities of product formation for various enzymes are shown in Fig. 4.

Of the proteases of different classes tested, only Neutrophil Elastase, Proteinase 3 and Porcine pancreatic elastase were able to hydrolyze the substrate into a product at a significant rate. This narrow specificity is similar to that observed for the paranitroanilide chromogenic substrate used in this study. As expected for an elastase with similar substrate preferences, Porcine Pancreatic Elastase (PPE) was also able to catalyze substrate hydrolysis at a high rate of the same order of magnitude as NE. Again, the selectivity of the peptide-linked nitroxide is similar to the one of the paranitroanilide chromogenic substrate bearing the same peptide. It is however irrelevant in the context of most inflammation diseases since PPE is synthetized as an inactive pro-enzyme and activated only in the intestinal lumen. Thus, the simultaneous presence of both enzymes is impossible except in pancreatitis where premature activation of PPE coexists with a strong inflammation. These experiments yielded similar results for isomers S and R.

3.2.4. **Relevance to inflamed lung situations**

To determine the relevance of this substrate for in vivo imaging of inflammation, NE detection was carried out using bronchoalveolar lavages derived from a mouse model of *Pseudomonas* pneumonia characterized by an acute pulmonary inflammation. Mice were *intra nasally* challenged with sterile PBS or containing *Pseudomonas aeruginosa* [21]. To assess the accuracy and specificity of NE detection, mice deficient in NE (NE-KO) or the three serine proteases namely NE, Proteinase 3 and Cathepsin G (3KO) were employed along with their Wild Type litter-mates (WT) [3]. Initial velocities were recorded by EPR after adding 1 mM substrate directly in the BronchoAlveolar Lavages (BALs) (Fig. 5).

As expected, infected WT mice BALs contained the maximal enzymatic activity. Interestingly, the activity in infected NE-KO mice samples dropped by 50% compared to the infected WT samples. Furthermore, 3KO lost 70% of the reference activity. Since Cathepsin G is inactive and Proteinase 3 active on this substrate, this additional activity decrease in 3KO can be confidently attributed to the absence of Proteinase 3. All control mice displayed an activity in the range of that corresponding to the control spontaneous dissociation. To further support our findings, prior addition of Batimastat, a broad spectrum matrix metalloproteinase inhibitor to infected BALs had no effect on activity measurements (data not shown). Thus, the detected activity stems exclusively from the neutrophil proteases NE and to a lesser extent from Proteinase 3. The apparent difference between the infected and uninfected 3KO samples is not statistically significant in this set of experiments. The slightly higher values for the infected 3KO could nevertheless be easily explained by some minor enzyme activities brought by the bacteria *Pseudomonas*. Pseudomonas elastase, however, cannot contribute as seen in Fig. 4.

Clearly, enzymatic activities in the setting of tissue inflammation can be detected by EPR in infected mouse BALs with this substrate. Significantly, hydrolysis of this substrate is due to active neutrophil proteases and hence represents a selective marker of inflammation.

3.3. **Images of elastase activity using Overhauser-enhanced MRI**

Recently, the discovery of nitroxide-based substrates undergoing strong electron resonance spectrum alteration upon enzyme action led to the concept of “Overhauser switch” [17,18]. Overhauser-enhanced imaging was proven possible *in vitro* and *in vivo*. Thus, the NE specific substrate was used as a potential polarizing agent through *in vitro* and
3.3.1. Properties of the substrate and the product as an OMRI contrast agent

The EPR irradiation frequency of the fourth line upfield was swept by tuning the cavity of the OMRI setup and the resulting MRI signal was plotted. The maximum signal enhancements were observed at distinct electronic EPR frequencies: 5425.6 MHz for the substrates $R^{-3}$• or $S^{-3}$• and 5414.4 MHz for the product $1•$ (Fig. 6) as predicted from the EPR spectra.

As for the EPR spectrometry study (cf. Enzymatic hydrolysis of the substrate), both lines are well separated and do not overlap. Linewidths are narrow enough to easily observe high signal enhancement in OMRI experiments. The full width at half maximum of the OMRI-derived EPR spectra in Fig. 6 was 7.4 MHz for the substrate $R^{-3}$• and 4 MHz for the product $1•$. Thus, linewidths in OMRI data agree with the results obtained by EPR spectrometry. Difference in linewidth values could be explained by the difference in the molecular weight of each nitroxide form (cleaved or uncleaved) as it acts on the tumbling rate and a probable contribution of the conformational change that is expected to modify the hyperfine coupling with the cycle and methyl protons. Moreover, it can be noticed that the product EPR signal amplitude increased about 1.5 times upon hydrolysis thus facilitating proteolysis detection.

As the frequency domain of EPR irradiation in this OMRI experiment is narrow compared to the linewidths, each nitroxide can thus be

**Table 2**

<table>
<thead>
<tr>
<th>Enzymatic Michaelis constants for the (R) and (S) substrate isomers.</th>
<th>$R^{-3}$•</th>
<th>$S^{-3}$•</th>
</tr>
</thead>
<tbody>
<tr>
<td>$K_m$ (μM)</td>
<td>15 (± 2.9)</td>
<td>25 (± 5.4)</td>
</tr>
<tr>
<td>$k_{cat}$ (s$^{-1}$)</td>
<td>14 (± 0.9)</td>
<td>16 (± 1.1)</td>
</tr>
<tr>
<td>$k_{cat}/K_m$ (s$^{-1}$ M$^{-1}$)</td>
<td>930,000</td>
<td>640,000</td>
</tr>
</tbody>
</table>

ex vivo OMRI experiments.
observed selectively with specific irradiation. On one hand, irradiating a sample with the product EPR frequency will give access to the enzymatic activity. On the other hand, irradiating at the EPR frequency of the substrate will give access to its bio distribution.

The $1^H$ longitudinal relaxivity $r_1$ was measured through a classical MRI experiment for the substrate $3•$ and the product $1•$ and were equal to $0.40 \text{s}^{-1}\text{mM}^{-1}$ and $0.42 \text{s}^{-1}\text{mM}^{-1}$, respectively. Those results are comparable to the relaxivity $r_1$ of Oxo-TEMPO ($0.5 \text{s}^{-1}\text{mM}^{-1}$) (unpublished results) which is characteristic of a water accessible electron.

The OMRI sensitivity at 0.2 T was investigated (Fig. 7). Maximum DNP factors reached $-26$ for the product at about 2 mM, and $-6$ for the substrate at about 1.4 mM. It should be noted that enhancement is higher for the product. This discrepancy might be the consequence of a lower EPR saturation efficacy of the substrate EPR line, since the electronic saturation is correlated to the nitroxide linewidth.

Fig. 5. Rate of product formation in bronchoalveolar lavages from unchallenged mice and mice infected by *Pseudomonas aeruginosa* (P.A.) for 24 h. 1 mM substrate was added extemporaneously. WT: wild type mice; NE-KO: mice Knocked-out for NE; 3KO: mice knocked-out for three neutrophil proteases. Control: spontaneous hydrolysis of the substrate. Significance bars are the result of an ordinary one-way ANOVA Tukey’s multiple comparisons test.

Fig. 6. Determination of the optimal excitation EPR frequencies for OMRI experiments: The EPR irradiation frequency of the fourth line upfield was swept and the resulting MRI signal was plotted. Overhauser signal enhancement of the substrate $R-3•$ (A) and product $1•$ (B) were fitted using a lorentzian model. The MRI $B_0$ field was 0.1936 T for the substrate and 0.1935 T for the product.

Interestingly, a DNP factor of $-3$ corresponding to an Overhauser enhancement of 2 (or to 200% contrast) remains for 0.09 mM of product (as inferred from Eq. (1) in the Material and methods section), which is a concentration compatible with future *in vivo* experiments. This result showed a very good sensitivity of the method as low substrate and product concentrations can be detected with high contrast.

### 3.3.2. Enzyme kinetics by OMRI in vitro

Since the substrate and the product can be detected by OMRI enzyme activity imaging was probed. Hence, the substrate was reacted with neutrophil elastase and the hydrolysis was monitored by OMRI. Fig. 8 shows relevant images acquired with the EPR irradiation set at the product or the substrate frequency as a function of time.

A maximum Overhauser enhancement of 5 for the substrate was obtained at the beginning of the reaction whereas a maximum enhancement of 8 for the product was obtained at the end of the reaction. The estimated catalytic constant by OMRI using the initial slope of the time-resolved Michaelis kinetics ($k_{cat} = 6 \text{s}^{-1}$) revealed a similar value than the one calculated by EPR (see Table 2). Thus this substrate is suitable for the detection neutrophil elastase activity by Overhauser-enhanced Magnetic Resonance Imaging. It is also an imaging method suitable to visualize the bio distribution of the substrate.

### 4. Discussion

Molecular imaging of enzyme activity by MRI is a long-sought-after tool. To achieve this, it was needed to produce a contrast and to trigger it specifically via enzyme activity. Since enzyme concentrations are mostly in the nanomolar range an amplification step was also necessary to overcome the gap of sensitivity with MRI which essentially produces images from the highly concentrated water protons. In this study high contrast was given by Overhauser-enhanced MRI in the presence of a nitroxide. The contrast was conditioned to enzyme catalysis by linking a specific peptide to a line-shifting nitroxide. Thus by choosing the EPR irradiating frequency of the “Overhauser switch” either the substrate or the product (hence the enzyme activity) would produce contrast. Furthermore, signal amplification naturally occurred from the enzyme turn-over as long as fresh substrate was present. The first approach was to target Neutrophil Elastase, a protease associated with numerous inflammatory diseases. After characterization, the substrate was successfully tested on samples from a *Pseudomonas aeruginosa* lungs infection.
The difficult but successful grafting of a chosen peptide on the shifting nitroxide core suggests that a new family of protease activity probe can be designed. Furthermore, the acetate enol ester [18] and the elastase-specific peptide enol ester have the same EPR spectrum and yield the same product after hydrolysis. Thus, the same instruments and the same settings will be valid regardless of the protease targeted. Expanding the targeted proteases by varying the peptide would allow exploring other pathologies like pancreatitis or tumors via their associated specific protease activity.

4.1. The MeO-Suc-(Ala)2-Pro-Val-nitroxide is a specific and fast substrate for elastase.

The specificity tests show that MeO-Suc-(Ala)2-Pro-Val-nitroxide is a fast substrate for Neutrophil Elastase and in a lesser extent for Proteinase 3. All other tested proteinases including serine proteinases and matrix metallo proteinases are ineffective. Particularly, the metallo elastase from Pseudomonas aeruginosa does not generate any product. Thus, with the irrelevant exception of pancreatic elastase, this substrate is a reliable marker of inflammation via neutrophil serine proteases. The
Michaels constants for elastase reveal a better substrate than its optically active paranitroanilide analog. In mouse BALs from the present acute inflammation model an activity from 1 nM of NE is detected. In human, BALs are estimated to dilute the epithelial lining fluid of about one hundred fold [38]. Thus, the concentration of NE in lungs of wild type infected mice would be 100 nM in vivo. In this situation, using the Michaels constants, a concentration as low as 75 μM of substrate (5 times the Kₐ) would generate 1.4 μM/s of product which would thus reach 140 μM in 100 s. Such a product concentration generates an OMRI contrast of 200% as deduced from the OMRI sensitivity plot. In vivo imaging of acute inflammation should then be possible within a short time provided that the substrate could be supplied quickly to the lungs prior to OMRI. In the case of cystic fibrosis concentrations of active elastase in the epithelial lining fluid are in the range of 2 μM even for patients with mild lung disease [39]. This is 2000 fold the lower limit of our method thus ensuring a fast and strong signal in a few seconds.

4.2. Towards a new tool first for research then for diagnosis

The first expected impact of this study is to provide a useful and very specific diagnostic tool for inflamed lungs. More specifically, the goal is to perform molecular MRI of any protease/inhibitor imbalance with a true 3D resolution firstly for Neutrophil Elastase but also Cathepsin G, Proteinase 3, MMP-12 and marginally for NSP4. It would then be possible to inventory the endangered areas in the lungs and later verify that a protective treatment with protease inhibitors has indeed inhibited the enzyme activity. This diagnosis at a molecular scale could be done prior to any anatomical alteration. Abnormal proteolysis would be visible thus at a much earlier stage of the disease when lung can still be preserved. For instance, in the pseudomonas aeruginosa infection model it was possible to monitor the inflammation while the lungs were reversibly altered. Ultimately it could be used as a monitoring tool for a personalized treatment until protease activity is effectively inhibited. All images were performed using the same setup as for in vivo imaging of mice published earlier. Thus, at shorter term, the method could be used as a pre-clinical tool to develop protease inhibition strategies for emphysema or cystic fibrosis using animal experimental models with a real-time monitoring of protease activity in vivo. To this end, studies are ongoing.

New diagnosis on human could be done using the presented nitroxide substrate and EPR. For instance, since EPR is able to perform on samples that are opaque to the visible light it could be used to detect enzyme activity in tissue samples such as biopsies. All OMRI experiments herein validated the use of the substrate MeO-Suc-(Ala₃)-Pro-Val-nitroxide as a specific proteolysis probe for OMRI. Future in vivo experiments of proteolysis imaging will be done to visualized pulmonary inflammation in situ. Application to human disease with OMRI will require further development. This stems from the EPR frequency that is about 650 times higher than NMR frequency. Consequently, at 0.2 T the electron resonance frequency is in the microwave range around 5.4 GHz. While it is possible to make mouse images this frequency is not suitable for larger animals because of low penetration depth. Interestingly, MRI at very low field is a currently active research area [40-44]. For instance at earth magnetic field the EPR frequency of nitroxides is in the range of several dozens of MHz, which allows convenient saturation of electron states and high penetration depths suitable for humans.

Acknowledgments

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